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- GB 1571629

 - GB 1520246
 - **GB 14794**6
 - GB 1478020
 - GB 1381872
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(54) Inhalation drugs

(57) A finely divided inhalation drug, e.g. sodium cromoglycate, comprises a therapeutically effective proportion of individual particles capable of penetrating deep into the lung, characterised in that a bulk of the particles which is both unagglomerated and unmixed with a coarse carrier, is sufficiently free flowing to be filled into capsules on an automatic filling machine and to empty from an opened capsule in an inhalation device. A proportion of the individual drug particles may have a spherical, collapsed spherical or ring doughnut shape.

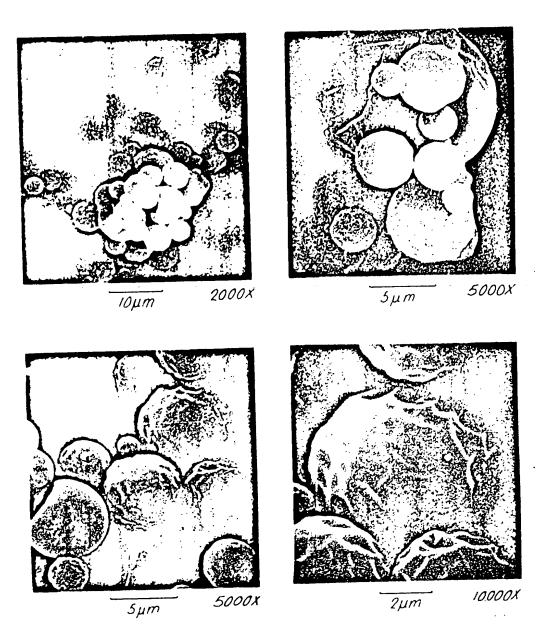


Fig.1.

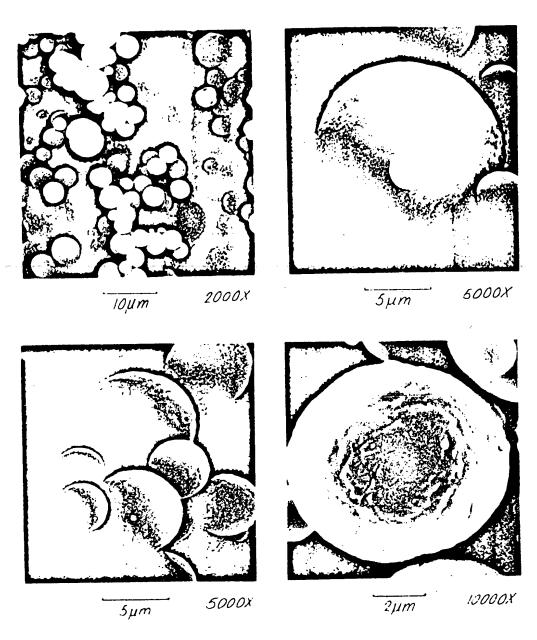


Fig.2.

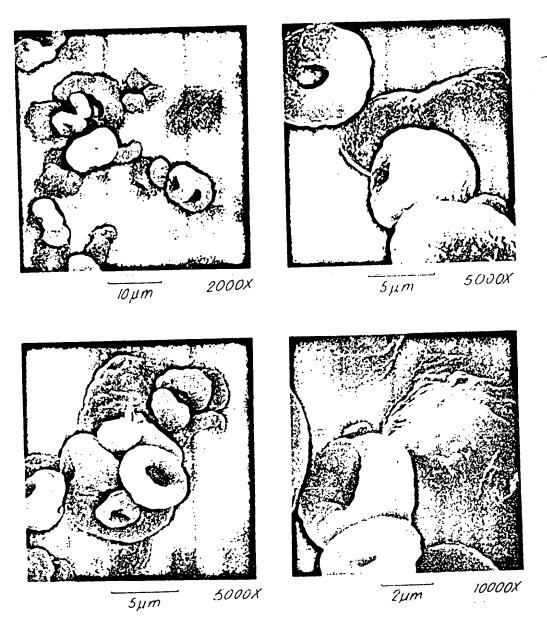


Fig. 3.

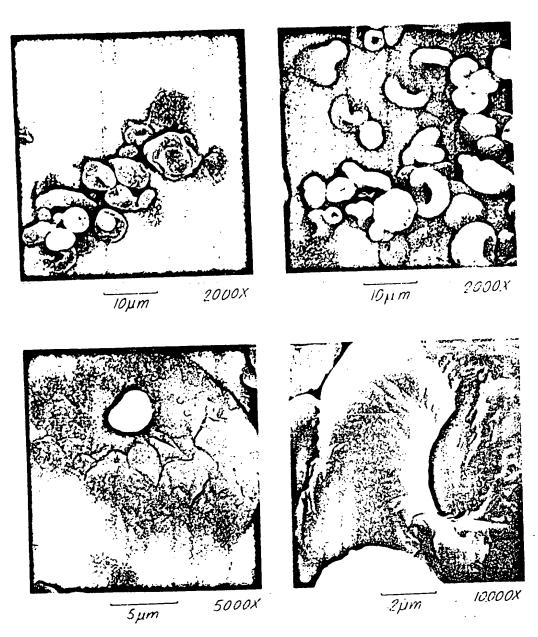


Fig.4.

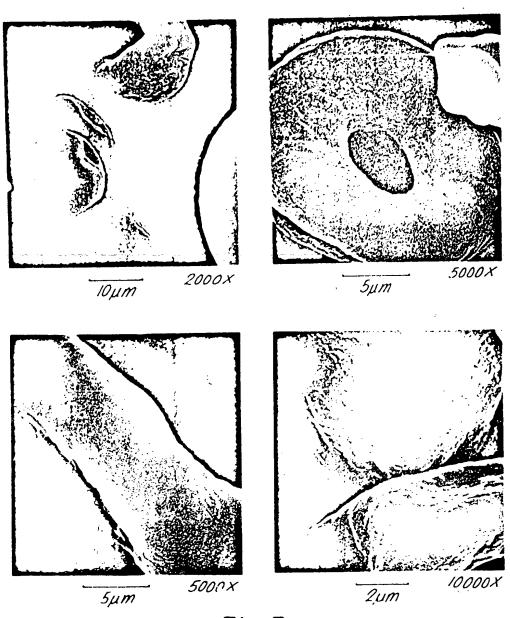


Fig. 5.

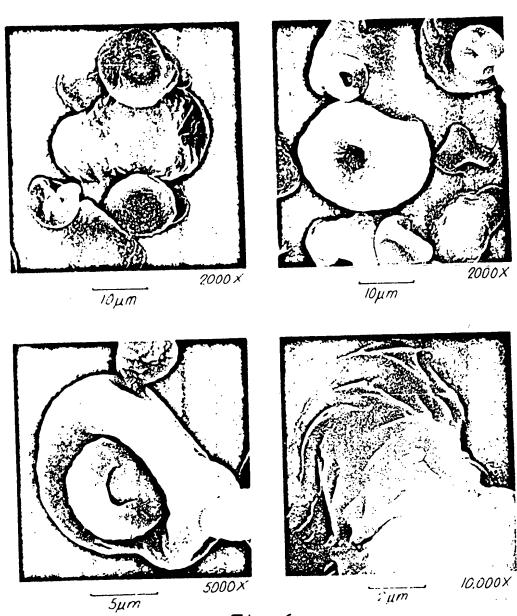


Fig.6.

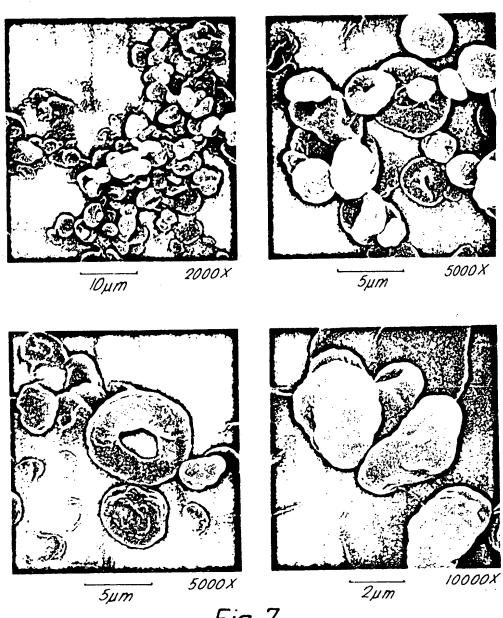
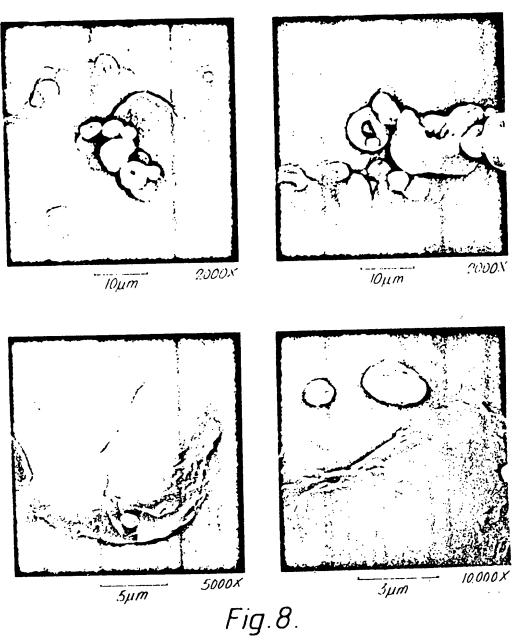


Fig. 7.



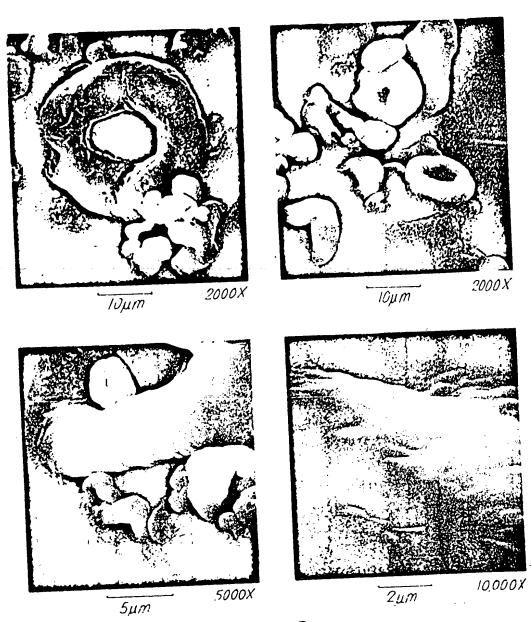
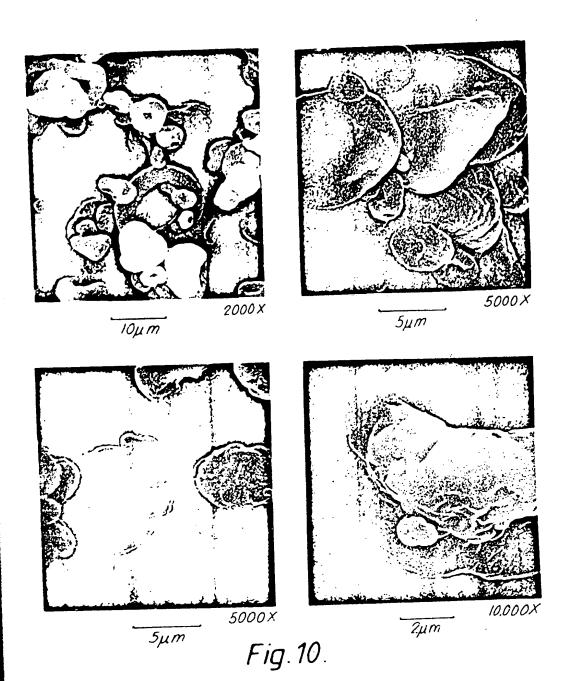


Fig.9.



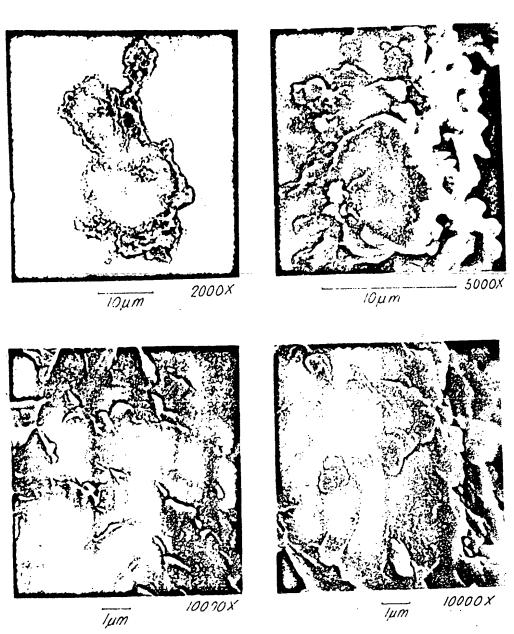


Fig.11.

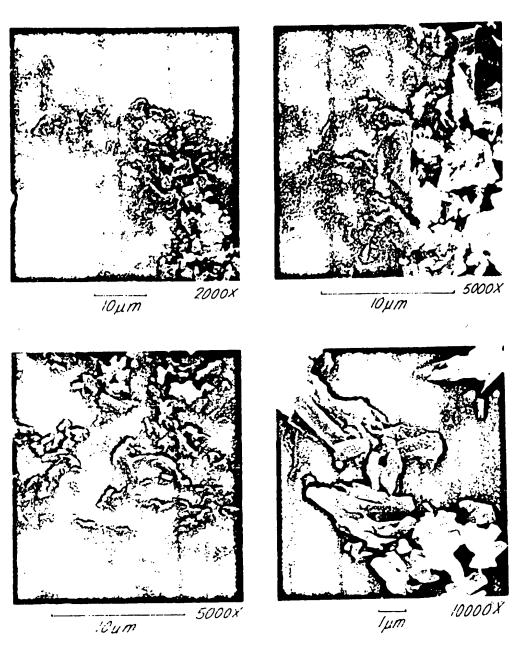


Fig.12.

SPECIFICATION

inhalation pharmaceuticals

This invention relates to a novel form of drug and to methods for its production and formulation. 5 In our British Patent No. 1,122,284 we have described and claimed an insufflator device for use in the administration of powdered medicaments by inhalation. With that device, and other devices, e.g. that described in British Patent Specification No. 1,331,216, and European Patent Application No. 813021839 a user inhales air through the device which causes a powder container mounted therein to rotate. Powder within the container is fluidised and dispensed into the air stream which is inhaled by the user. For optimum 10 dispensing it has been found that the powdered medicament particles should be comparatively free-flowing and yet should have an ultimate particle size of less than about ten microns to ensure adequate penetration of the medicament into the lungs of the user. These two requirements are prima facie mutually exclusive, since such fine powders are not usually sufficiently free-flowing. It has in the past been found that this 15 problem can be mitigated or overcome, e.g. as described in US Patent 4,161,516, by forming the powdered medicament into small soft pellets or soft granules. Both soft pellets and soft granules will fluidise satisfactorily within the container and yet are of sufficiently low internal coherence to break up into finer particles of medicament of a therapeutically effective size in the turbulent airstream around the outside of the container. However the procedure of forming the micronised drug into soft pellets or granules is both 20 difficult and expensive. An alternative means of getting the fine particles to flow and disperse satisfactorily 20 has been to mix them with a coarse carrier, e.g. coarse lactose (see US Patent No. 3,957,965). However with all pharmaceuticals it is desirable to use as pure a form as possible (inter alia to avoid any possible adverse reactions by the patient to the excipients) and the presence of the coarse carrier is not therefore desirable. Furthermore the mixing of the fine drug with the coarse carrier involves the extra expense of the carrier, the 25 possibility of segregation of carrier and drug during transport and storage, and extra process steps which add to the cost of production. Production of both the pelletised material and the blend of fine material with the coarse carrier involves the initial step of micronising the drug. Sodium cromoglycate has been made, for blending with lactose or agglomeration into soft nearly spherical pellets and administration by inhalation, as a micronised dry powder and in this form consists mostly of rods or lath-shaped crystals. In both the 30 pelletised and blended material energy is needed to break up the pellets or to separate the fine drug from the coarse carrier before or during inhalation. Thus in many instances it has also been found that the amount of drug which is available as fine particles in the air stream is dependent on the rate at which air is passed through the inhaler (i.e. the amount of energy imparted to the formulation). This can be particularly disadvantageous when the drug is used to treat patients suffering from conditions affecting their ability to 35 Thus for many years the production of drugs in a form in which they can flow easily (and therefore be filled 35 breath. readily into capsules) while at the same time being of a sufficiently small particle size to penetrate deep into the lung has presented a problem which has only been capable of resolution by means of complex We have now found particles which can penetrate deep into the lung and yet which are sufficiently free 40 flowing to be filled into capsules, and otherwise manipulated, without mixing with a coarse diluent or formation into soft pellets or granules. We have also found that these particles can disperse well from an inhaler at both low and high air flow rates, thus, in certain circumstances, improving consistency of capsule emptying. Furthermore we have found that the new particles can, in general, be coarser than those of the 45 prior art while giving an equivalent proportion of particles capable of penetrating deep into the lung. 45 According to the invention we provide a finely divided inhalation drug comprising a therapeutically effective proportion of individual particles capable of penetrating deep into the lung, characterised in that a bulk of the particles which is both unagglomerated and unmixed with a coarse carrier, is sufficiently free flowing to be capable of being filled into capsules on an automatic filling machine and to empty from an 50 opened capsule in an inhalation device. According to the invention we also provide a drug in finely divided and unagglomerated form, wherein a substantial proportion of the individual drug particles have a spherical, collapsed spherical, i.e. where one or both sides of the sphere appear to have been pushed inwards, or toroidal shape, i.e. the shape of a ring doughnut. The ring doughnut shapes may have a hole through the middle or may have a thin membrane 55 filling the hole. In certain cases a population of two or more of spheres, partially collapsed spheres, fully 55 collapsed spheres and ring doughnut shapes is found. The individual particles should be as rounded and smooth as possible to enable them to be carried easily In an air stream and to flow readily on capsule filling machines. We prefer the majority of the particles not to have sharp or broken edges, and for the particles themselves to be mechanically strong so that they do not

break during encapsulation or on their passage from the capsule to the lung. Thus we prefer to avoid hollow shell particles. We particularly prefer a proportion of the particles, especially when the drug is sodium cromoglycate, to be toroidal in shape. In general to shape of the particles is unrelated to particle size. We have also found that in general the particles have smooth cleavage planes, are relatively non-porous and are c'uniform density through each particle. With respect to their strength the particles of the present invention are strongly differentiated from the prior art soft pellets and granules, and with respect to their shape they

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are strongly differentiated from the prior art micronised material. A low particle density in the material is indicative of fragile particles and is, in general, to be avoided. We profer the particles to be as uniform as possible in all respects.

The surface texture of the particles will vary according to the particular drug concerned and the techniques used to produce the particles, and can vary from a highly convoluted (brain like) structure to a random fluffy or to a smooth texture. In general we prefer to avoid highly convoluted surface textures.

The roughness of the surface of the particles can be determined by measuring the total surface area of the particle by the Brunauer, Emmet and Teller (BET) method (British Standard 4359 (1969) Part 1) and comparing this with the envelope surface area of the particles as measured by permeametry (Papadokis M. (1963), Rev. Mater. Construct. Trav. 570, 79-81).

We prefer the permeametry: BET ratio to be in the range 0.5 to 1.0, preferably 0.6 to 1.0 and more preferably 0.7 to 0.97 (note a ratio of 1.0 represents a perfectly smooth particle). By way of contrast prior art micronised drugs, e.g. micronised sodium cromoglycate, have a permeametry: BET ratio of about 0.32.

We prefer the particles of the invention to be as strong and as dense as possible. The particle density of the particles (as oppossed to the bulk density) may be measured by

a) the petroleum ether method in which a known weight (25g) of powder is weighed into a measuring cylinder, a known amount of petroleum ether (50ml) is added and the mixture shaken until all the powder is suspended. The inner walls of the measuring cylinder are washed with a small amount of petroleum ether (10ml). Knowing the weight of powder used, the volume of petroleum ether added and the final suspension volume, the particle density can be calculated. or

b) the air pycnometer method in which a given amount of powder is placed in a chamber which is hermetically sealed. The volume of the chamber is gradually reduced by a moving piston until a specified pressure is reached. The position of the piston indicates the volume of the powder particles, hence the particle density can be calculated.

We prefer the particles, e.g. of sodium cromoglycate, to have a particle density according to the above methods of from about 1.3 to 1.7 and preferably from 1.3 to 1.6 g/cm³.

The micronised material, e.g. sodium cromoglycate, of the prior art has a loose bulk density of about 0.21 g/cm³ and a packed bulk density of about 0.29 g/cm³. In measuring loose bulk density a suitable amount of powder (40g) is poured, at an angle of 45°, into a measuring cylinder (250ml). The volume occupied by the powder in the measuring cylinder when related to the original mass of powder provides the measure of "loose bulk density". If the powder, in the cylinder, is tapped or jolted, e.g. using the Engelsmann Jolting Volumeter, until a stable volume is attained (500 jolts) then the lower volume after jolting when compared with the original mass of powder provides the measure of "packed bulk density".

It is also known, e.g. from British Patent Specification No. 1,549,229 that hard granules of sodium cromoglycate of particle size 60 to 200 microns (measured by sieving) can have higher bulk densities than the micronised material. However these hard granules were not designed for, and indeed would be unsuitable for, inhalation. Surprisingly we have found that the particles of the present invention have a higher bulk density than micronised material, e.g. micronised sodium cromoglycate. We prefer the particles of the present invention to have a loose bulk density of greater than about 0.3 g/cm³, preferably of greater of than 0.35 g/cm³, more preferably of from 0.35 to 0.5 g/cm³, and most preferably 0.35 to 0.4g/cm³; and a packed bulk density of from about 0.4 to 0.75 g/cm³ and preferably of from 0.55 to 0.6g/cm³. The bulk densities of materials are, in general, relative independent of the particular material used, but are dependent on the shape, size and size distribution of the particles involved.

We prefer the particles of the invention, when they comprise sodium cromoglycate and are intended for
45 administration as a dry powder in, for example, a gelatine capsule to have a moisture content of from 5 to 14,
45 and preferably from 8 to 11% w/w. Before filling into the capsule the powder will tend to be at the lower end
of the moisture range, and after filling to be at the upper end of the range. Sodium cromoglycate powders
according to the invention may also be made containing very low, e.g. less than 1%, or preferably less than
0.5%, w/w, quantities of water. These very dry powders may be used in pressurised aerosol formulations.
50 The water contents in this specification are those measured by drying a small sample (1 to 2g) for 15 hours at
105°C in a vacuum oven (less than 5 mm Hg) in the presence of phosphorus pentoxide.

Examples of suitable medicaments include those used for the inhalation treatment of allergic airway diseases such as pharmaceutically acceptable salts of 1,3-bis(2-carboxychromon-5-yloxy)propan-2-ol; bronchodilators, e.g. isoprenaline, salbutamol, fenoterol, terbutaline, reproterol etc and salts of anyone thereof; antibiotics, e.g. tetracycline; steroids, e.g. beclomethasone dipropionate; enzymes; vitamins and antihistamines. If desired a mixture of medicaments, for example a mixture of sodium cromoglycate and a broncholdilator, such as isoprenaline, terbutaline, fenoterol, reproterol or a salt of any one thereof, may be used. Where a highly active medicament is used which requires a small unit dose the individual particles may comprise the active ingredient together with a suitable diluent, e.g. lactose. The incorporation of the diluent in the particle avoids the possibility of segregation which is possible when individual fine particles of active ingredient are used with separate coarse particles of diluent.

We prefer that at least 50% by weight a: . preferably more than 90%, of the drug particles are of less than 60 microns, more preferably of less than 40 microns, most preferably of less than 20 microns and especially of less than 10 microns, e.g. less than 8 microns in diameter. We particularly prefer at least 50% of the particles to be of 2 to 6 microns in diameter, In general the smaller the mass mean diameter of the material

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the higher will be the dispersion of the material, as measured by the test of Example A(a).

Material according to the invention, e.g. sodium cromoglycate, having a median diameter of from 10 to 15 microns can, because of the enhanced aerodynamic properties of the particles, be equivalent in emptying and dispersion properties (see Example A) to micronised (i.e. sub 10 micron) material which has been formed into soft pellets as described in US Patent 4,161,516 or blended with coarse lactose, as described in US Patent 3.957.965.

The particle sizes in this specification are those measured with a Coulter Counter TA11 used in a standard laboratory environment, or the pipette centrifuge. In measuring particles sizes with a Coulter Counter, the sample to be analysed is dispersed in an electrolyte into which dips a glass tube. The glass tube has a 50 to 400 micron hole through the wall thereof with electrodes mounted on either side of the hole in the tube wall. The tube is immersed sufficiently for the hole and electrodes to be submerged in the liquid. The suspension is made to flow through the hole in the glass tube and as each particle passes through the orifice it displaces its own volume of electrolyte, thus changing the resistance across the hole. This change in resistance is converted into a voltage pulse with an amplitude proportional to the particle volume. The pulses are fed to an electronic counter with an adjustable threshold level such that all pulses above the threshold are counted. 15 By setting the threshold level at different values it is possible to determine the number of particles falling within given size ranges and thus the proportion of particles in a sample which fall outside a desired particle size range. The Coulter Counter measures the volume of a sphere having the same volume as the unknown material, i.e. it measures a volume diameter.

In measuring particles by the pipette centrifuge (Christison Scientific Equipment Limited) the powder is suspended in a suitable liquid (e.g. n-butanol). The suspended sample is put in a constant speed centrifuge. Samples are withdrawn from the centrifuge at selected time intervals. The level of solids in each sample is measured (normally by drying) and the average diameter calculated using an equation derived from Stokes Law (Particle Size Measurement Published by Chapman Hall 3rd Ed. Dr. T. Allen, page 377 et seq.). The 25 pipette centrifuge measures a mass, or Stokes, diameter.

The Coulter counter (with a 100 micron hole) is able to measure particle sizes of from about 2 to 40 microns and the pipette centrifuge is able to measure particle sizes down to about 0.2 microns.

According to the invention we also provide a process for the production of finely divided drug, which comprises atomising and drying a solution of the drug and collecting some or all of the particles which are 30 below 60, preferably below 40, more preferably below 20 and especially below 10 microns in diameter. The particles are preferably of the sizes given above.

Spray or flash drying of materials is well established as a drying technique in the food and other industries, but is scarcely used at all in the pharmaceutical industry. Thus spray drying is routinely used in the poduction of coarse particle products such as dried milk, instant coffee and dextran. The use of spray drying techniques to produce very fine powders is not conventional and is unknown in the pharmaceutical field, the normal technique for producing such fine powders being to make, and then micronise, a crystalline drug. The use of a spray drying technique is advantageous in that it is adapted to suit large batch productions, thus decreasing the amount of quality control required and also in that it may remove the need for recrystalisations and micronisation to get the drug into the desired form.

Any suitable form of atomiser can be used. Atomisation results from an energy source acting on liquid bulk. Resultant forces build up to a point where liquid break-up and disintegration occurs and individual spray droplets are created. The different atomisation techniques available concern the different energy forms applied to the liquid bulk. Common to all atomisers is the use of energy to break-up liquid bulk. Centrifugal, pressure and kinetic energy are used in common forms of atomiser. Sonic and vibratory atomisers are also used. Specific atomisers which may be mentioned include rotary atomisers, e.g. those involving vaned wheels, vaneless discs, cups, bowls and plates; pressure atomisers, e.g. those involving pressure nozzles, centrifugal pressure nozzles, swirl chambers and grooved cores; kinetic energy or pneumatic atomisers, e.g. those involving two or three fluids, or internal or external mixing; and sonic energy nozzles, e.g. involving sirens or whistles. We prefer to use kinetic or pneumatic energy atomisers 50 particularly two fluid pressure or syphon or sonic nozzle atomisers. In general two fluid pressure nozzles tend to produce powders having more desirable characteristics than two fluid syphon nozzles and two fluid pressure nozzles also tend to give more reproducible results and use less energy.

The atomiser can be used in a spray or flash drying apparatus.

The conditions of operation of the apparatus and storage of the solution (e.g. pH and temperature) should 55 clearly not be such as to degrade the drug, or introduce impurities, or biological contamination, into the

drug. The spray drying apparatus preferably comprises the atomiser, a main chamber, one or more (e.g. two) cyclones, a bag filter and, if desired or necessary to maximise recovery, a terminal wet scrubber or electrostatic precipitator. The particle collection system is designed to capture the desired size range of 60 particles and also to maximise the yield. All over and under size material may be recovered and recycled or put to other uses.

The solution of the drug may be in any suitable "ulvent, e.g. water from a water soluble drug. The concentration of the drug in the solvent may vary over a wide range, e.g. in the case of sodium cromoglycate from 1 to 25, preferably 5 to 20, and especially 10 to 15 % w/v. In general we prefer to use a high concentration of drug as the volume and energy requirements of the atomisation and drying process are

thereby diminished. To avoid possible blockage of the atomisation device and to avoid the incorporation of unwanted impurities it is desirable to filter the solution immediately before it is passed to the atomiser. The particle size of the product tends to increase with concentration, but not rapidly, and in general concentration is not controlling with respect to particle size.

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The temperature of the air inlet and outlet to the spray drier main chamber may vary over a wide range (the range being dependent on the product being dried, the solution through put and the final moisture content required) and suitable temperatures may be found to suit each drug and solvent by simple routine experiment. In the case of aqueous solutions (of for example sodium cromoglycate), we have found that an air inlet temperature of from 160° to 350°C, preferably from 180° to 230°C, and an outlet temperature of from 10 70° to 250°C and preferably of from 70° to 120°C are suitable.

The temperature of the solution to be fed to the spray drier will vary with the drug and the solvent to be used. In general we prefer to use a temperature at which the solution can be stored for a long period in large batches without degradation. As high a temperature as possible comensurate with stability is desirable to reduce solution viscocity and provide energy to the drying process.

The air flow rate, direction into the spray drier, the temperature of the air and the rate of feed of solution to the spray drier can be optimised by simple experiment. All of the parameters in the spray drying process interrelate and can be adjusted to produce the desired product.

Gases other than air, e.g. nitrogen, can be used if desired. The use of an inert gas will be advantageous when an inflamable solvent or a readily oxidisable drug is used. The gas used, e.g. air or nitrogen, may, if 20 desired, be recycled to avoid loss of entrained drug and/or to conserve energy and the inert gas.

The particle size of the product will be set by the concentration of the feed solution, the rate of feed to the spray drier, the means of atomising the solution, e.g. the type of atomiser and the pressure of the air, and solution to be dried, the temperature and temperature gradient within the drier and, to a small extent, the air flow in the drier. The particle size and air fow will then dictate where the desired product is collected and the

The particle size of the product tends to remain fairly constant with liquid flow rate through the atomiser, 25 means of collection. but to decrease the increasing air pressure up to a limiting pressure, e.g. of about 11Kg cm⁻². The range of air pressure suitable will naturally depend on the atomisation device used, but we have found that air pressures of from about 2Kg cm⁻² to 11KG cm⁻² are in general effective, e.g. with a 0.4mm orifice syphon 30 two fluid nozzle. In order to achieve reproducible results we prefer to maintain a constant air flow to the dryer and appropriate air flow control devices may be used if desired.

The cyclone or cyclones used to collect the dried particles are of conventional design, but adapted to collect finer particles than is normal. Thus the pressure differential across the cyclones, the combination of two or more cyclones and the design of the particular cyclones used may be adjusted to enable capture of 35 the fine particles. The bag filter used to collect the finest material is of conventional design and is readily available. The filter medium within the bag filter preferably has a high capture efficiency for particles of approximately 0.5 microns in diameter and greater. A particularly suitable medium is a polytetrafluoroethylene membrane supported on a polypropylene or polyester cloth, e.g. a needle felt cloth. Any electrostatic precipitator, or wet scrubber, used will also be of conventional design.

The product may be classified, e.g. sieved or air classified, to remove over and under sized material. The over and under sized material may be recycled or used for other purposes.

The final product may be put up in any suitable form of container such as a capsule or cartridge. Where it is desired to use the product in association with other ingredients such as colourants, sweeteners or carriers such as lactose, these other ingredients may be admixed with the particles of the invention using 45 conventional techniques or may be incorporated in the solution to be spray dried. We prefer the particles of the invention to contain medicament and water only. Mixtures of two or more different particles according to the invention, e.g. of sodium cromoglycate and a bronchodilator, such as isoprenaline sulphate or tertbutaline sulphate, may be made and filled into suitable containers.

According to our invention we also provide a method of application of a medicament, e.g. sodium 50 cromoglycate, to a patient by way of inhalation, the medicament being dispersed into an air stream, characterised in that an opened, e.g. pierced, container, e.g. capsule, containing particles according to the invention is rotated and vibrated in an air stream which is inhaled by the patient. The rotation and vibration may conveniently be produced by any one of a number of devices, e.g. the device of British Patent Specification No. 1,122,284.

The particles according to the invention may also be used in pressurised aerosol formulations (together with propellant gases, e.g. a mixture of two or more of propellants 11, 12 and 114, preferably with a surface active agent, e.g. sorbitan trioleate) or may be formed into soft pellets, e.g. as described in US Patent Specification No. 4,181,516, or may be used for application to the skin. Sodium cromoglylcate is known to be of use in the treatment of a wide variety of conditions, e.g. asthma and hay fever.

From another aspect the invention also provides a capsule, cartridge or like container containing particles according to the invention, optionally in association with other particles. We prefer the container to be loosely filled to less than about 80% by vr ime, preferably less than about 50% by volume, with the particles of the invention. The particles are preferably not compacted into the container. We prefer the container, e.g. capsule, to contain from 10 to 100 mg, e.g. about 20mg, of the particles.

The invention will now be illustrated by the following Examples in which all parts and percentages are by

weight unless otherwise stated. **EXAMPLE 1** The active compound (A) was dissolved in a solvent, normally water, to a concentration B (% w/v). This 5 solution flowed under pressure or vacuum to the atomiser. At the atomiser the solution temperature was normally greater than 50°C. Conditions of atomisation (C) and of droplet drying (D) were preset and remained constant throughout the run. The powder was captured in the drying chamber, in two cyclones (firstly a Vantongeren Buell AC 130 cyclone of diameter 22 cm and height 74 cm and secondly a high efficiency Stairmand formula cyclone of diameter 14 cm) and finally in a bag filter which had as the filter 10 media polytetrafluoroethylene lined polypropylene. At the end of each run the contents of each collection 10 vessel was weighed (E) and sized (F) (Coulter Counter Model TA11). a) Varying active ingredients Using a concentration (B) of 10% w/v in water, and atomisation conditions (C) a pressure two fluid nozzle (0.4mm orifice), a solution flow rate of 65ml min⁻¹ and an atomisation pressure of 27×10^{2} Kg m⁻² the 15 15 results shown in Table 1 were obtained. Note - Electron micrographs (see Figures 1 to 4) showed. Salbutamol Sulphate - smooth spheres Terbutaiene Sulphate - "orange peei" spheres Isoprenaline Sulphate - smooth spheres 4,6-Dioxo-10-propyl-4H.6H-pyrano[3,2-g] pyran-2,8-dicarboxylic acid disodium salt "orange peel" spheres 20 with surface cracks Sodium Cromoglycate) "doughnut", spheres and other active ingredients) collapsed spheres 1 Sodium Cromoglycate/ 25 25 b) Varying atomisation Techniques Active ingredient (A) - Sodium Cromoglycate. Conditions used and results obtained are given in Tables 2 and 2a. - CT (London) Ltd. CT Type J1A 16/50 (4mm orifice) Two fluid syphon nozzle - CT (London) Ltd. CT Type J11 Two fluid pressure nozzle 30 - Ultrasonics Ltd, 035 H Sonicore nozzle Ultrasonic nozzle - Delevan Ltd - Swirl Air Nozzle Type 32183-1 Swirl Air nozzle c) Variation of powder collection techniques ine powder is collected in the drying chamber, cyclones and a bag filter. 35 Active ingredient A · Sodium Cromoglycate. Conditions used and results obtained are given in Tables 3 and 3a. Powder Capture Equipment - 13 cu ft (give metric equivalent) Main chamber (MC) size - Stairmand High Efficiency Cyclone (Diameter 14cm) Cyclone A - Vantogeren Buell AC 130 Cyclone (Diameter 22cm, Height 74cm) 40 ~Cyclone B - Stairmand High Efficiency Cyclone (Diameter 11.9cm) Cyclone C - 1.86 M² polytetrafluoroethylene lined polyester Bag Filter (BF) d) Variation of droplet drying time Droplet drying time is dependent upon both the temperatures used in drying, i.e. air inlet temperature, the 45 residence time in the drying chamber (normally this is as a result of drying chamber size) and level of evaporation required. Residence time can be changed by modifying the drying air flow rate but this results in a significant change in efficiency of capture within the latter cyclones. Table 4 indicates the range of drying conditions used. Increased residence time (i.e. slower drying) produced improved particles with improved 50 performance. Electron micrographs of a selection of the above powders are shown in the accompanying Figures. Figures

11 and 12 are electron micrographs of, respectively pelletised sodium cromoglycate, and micronised sodium cromoglycate and are included for comparison purposes only. In each of Figures 1 to 12 the magnification

and an approximate scale is given.

TABLE 1

\$ 3	Run No Artice Instruction (A)	Drying C Inlet Temp.	Drying Conditions (D) Inlet Outlet Temp. Temp.	Air Flow Rate	Main Chamber	Powder Recovered E/F Cyclone Cyclone B A	overed E/F Cyclone A	Electron Micrograph
į		ပ္	ပ္	E .		micron	diameter	
÷	Sodium Cromoghycate	2 6	8	0.034	2.0/-	80.7.5	18/3.4	
~	Terbutalene Sulphate	202	102	0.034	+	83/4.3	17/4.0	1 (B cyclone)
ಈ	Saibutamol Sulphate	8	501	0.034	÷	78/4.1	1.522	
4	Isopreneline Sulphate	201	8	0.034	Ŕ	34/6.5	3333	
4	4,6 Dlaxo-10-propyl- 4H,8H-pyrano(3,2-g) pyran-2,8-dicarboxylic acid disodium selt	200	801	0.034	7/16.5	786.2	154.1	2 (B cyclone
¢	Sodium Cromoglycate (100)/ Terbutalene Sulphate (0.522) w/w	200	101	0.034	. .	756.6	17/3.6	ю
۲.	Sodium Cromoglycete (100)/ Sulbutamol Sulphete (0.522) w/w	22	88	0.034	-/11	587.4	25/4.2	
ಪ	Sodium Cromoghyzate (100)/ laopranaline Sulphate (0.522) w/w	505	95	0.034	13/19.0	75.7.0	12.3.2	•
ದ	Suibutamol Suiphate* (1.6)/ Lactose (100) w/w	200	<u>,</u>	0.034	-//		93.7.8 (cyclone C)	

*Cyclone configuration changed to MC/C/BF.

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		Atomiestic	Conditions	0	Drying Co.	Drying Conditions (D)	_	Power Rec	Power Recovered E/F				
		Solution	Solution	Atomisation	Inlet	Outlet		Main	Cyclone	Cyclone		Electron	
Ž Š	Run Atomiser No. Type	S S S S S S S S S S S S S S S S S S S	Conc · Feed Rate Pre- % w/v Ls ⁻¹ ×10 ⁻³ Kgr	Pressure Kgm ⁻ ×10³	် မ (၁)	င် ဧ ရ	7. s. m		micron median	volume diameter		Figure No	
ರ	Slotted Disc	10	0.57	23000	230	¥.	90.03	•	91/15	95.2		5 (B cyclone)	
=	Slotted Disc	9	0.48	Ę	214	8	0.034	Ś	22/877	2/4.0		•	
2		9	0.70		220	118	0.034	Ŕ	65/17	34.3			
<u>.</u>		5	0.50		215	121	0.034	21/24	7.71/27			6 (B cyclone)	
#		G	0.33	150.7	238	125	0.034	1/-	19/4.5	31,2.8	\$		
بم		8	1.33	150.7	5 2	ま	0.034	26/15.5	127.4	62/3.1			
5		5	0.90	56.4	210	8	9.034	-/.	70.8.5	233.0			
7.		2	9.63 83	105.7	225	113	0.034	ኔ	34/4.7	31/2.9	30/2.1		
Ę	Two Fluid		0.37	28.2	<u>8</u>	132	0.034	873	62/6.8	303.7			
Ę.		5	0.33	28.2	92	88	0.034	12/-	17.9.2	11,3.5			•
Ŕ		2	1.52	18.3	210	호	0.034	24.	74/16.0	2/4.0		·	
2.		2	0.42	39.5	533	137	0.034	\$25 \$25	53/10	33/3.4	9.30	7 (A . cyclone)	-
ä	Two Fluid	5	1.33	36.6	502	88	0.034	13.	77/10.5	10/3.2			
ដ	Pressure Nozzie 5mm orifice	5	1.17	21.1	502	8	0.034	12.	79/9.2	9/4.2			
75	. Ultresonic Nozzle	5	1.47	35.2	210	83	0.034	ò	82/9.6	12/3.3		co	
% :	26. Swirt Air	51	1.17	49.3	5	8	0.034	5	79/14.5		ထံ	ത	
ž	Nozzie	Fet?	ber contents sl	Chamber contents showed incomplete drying.	te drying.								

-		Atomisation Conditions (C) SolutionS	nditions (Solution	ditions (C) Solution Solution	Atomi-	Dryir In is t	Drying Conditions (D) let Outlet Air Flow	g Conditions (D) Outlet Air Flow	Main	Powder Re Cyclone	Powder Recovered (E/F) Cyclone Cyclone Cyclone Bag	F) Cydone	Beg
	No. Capture Equipment	Atomiser	Conc	Feed Rate	sation Pressure	Temp.	Temp.	Rate	Chamber	<	B Volume	ပ	Filter
	Configuration	Type	**	Ls-1×10-3	Kgm ⁻² ×10³	ပ္	ပူ			median	diameter	microns	
	26. MCA8/8F	Two Fluid Syphon Nozzle	01	1.17	105.7	210	8	0.034	<i>સં</i>	87/9.6	10/4.2		
ij.	MC/BF	Nozzłe	5	1.27	105.7	215	88	0.034	1417				86.5.2
	MC/B/A/BF	Nozzie	5	0.88	105.7	218	112	0.034	ė	402.9	35/6.4		222.0
	MCBF	Two Fluid	6	1.5	18.3	8	8	0.034	50.				50/13.5
	MCBF	Nozzie 4mm	5	0.42	33.8	6	120	9.034	\$223				96/5.2
3.	MC/B/A/BF	Orifice	5	1.52	18.3	210	Š	0.034	24.	3/4.0	73/16		
	MC/CBF		5	6.0	35.2	2	8	0.034	11/-			86/6.5	ર્જ
	MCBF	Two Fluid Pressure	5	1.73	16.2	85	7.	0.034	-/19				39/14
	34. MCB/ABF	Nozzłe Smm	5	1.16	21.1	88	8	0.034	12⁄-	9/4.2	289.2		
Ŕ	MC/C/8F	Orifice	5	1.23	26.8	222	102	0.034	. 5			8 5 6	

TABLE 4

		Atomisation	Atomisation Conditions		Drying C	Drying Conditions			
ž Š	Atomiser Type	Solution Conc.	Solution Feed Rate	Atomisation Pressure	Inlet Temp.	Outlet Temp.	Air Flow Rate	Electron Micrograph Figure	
		% %	Ls-1×10-3	Kgm ⁻² ×10 ³	ပူ	ပူ	1-8-E		
ø	Two Fluid	8	1.67	176.2	<u> 78</u>	88	0.034		
33.	Syphon Nozzle	S	0.48	55.0	345	%	0.034		
· 8	Two Fluid	0	0.67	35.2	308	122	0.034	10 (1st cyclone)	
	Nozzie 4mm				•				
æ	Orifice	0	1.28	23.3	140	8	0.034		

EXAMPLE 2

The experiment was carried out using a spray drier which had a main chamber and a single cyclone. (Main the experiment was carried out using a spray drier which had a main chamber and a single cyclone, (Mai chamber 0.37m³, cyclone Stairmand High Efficiency design with diameter 119mm). Atomisation was achieved using a two fluid pressure nozzle with orifice diameter 0.44mm. With an aqueous sodium 5 cromoglycate feed solution concentration of 15 % w/v, an air flow rate of 0.034M³s⁻¹ and other conditions set out in Table 5, the results shown in Tables 5, 5s and 5b v:srs obtained. Table 5b gives test results when the powders produced according to this Example have been filled into hard gelatine capsules.

					TABLE 5	,			*.	10	
10		Atomisation Co	nditions (C)	Dry	ing Cond	itions (D)	Powder F	Recovered E	UF \		
	Run	Solution Feed	Atomisatio	n inle	t	Outlet	Main	Cyc	clone		
15	No.	Rate	Pressure	Ten	np	Temp	Chambe	r		15	
		Ls ⁻¹ ×10 ⁻³	Kgm ⁻² ×10	, .c		*C	%/Micro Diamete	n Volum e N r	ledien		
20	40.	1.33	27.5	190)-200	70-80	33/-	67/	13.0	. 20	
	41.	1.58	21.2	220)-230	85-95	40/-	60	14.7		
	42.	1.43	25.4	199	5-200	80-90	20/-	80	/13.8	25	
25	43.	1.50	24.0	199	5-204	75-85	33/-	67	/13.7	÷	
	44.	1.58	22.6	190	0-200	70-80	36/-	64	/14.0		
30	45.	1.50	24.0	19	5-205	80-90	34/-	66	/16.5	30	
					TABLE !	5a					
				-	Powder o	iata				35	
35	35 Test			Run Nur 40	nber 41	42	43 44		45		
	M	Moisture % w/w			9.7	8.4	9.8	9.8	9.5	40	
40		Particle Size: Volume median diameter microns % w/w 6 microns			14.7	13.8	13.7	14.0	16.5		
					8	9	8	8	7		
45	%	w/w 30 microns		4	7	. 8	8	8	15	45	
	L	oose Bulk Density	g/cm³	0.39	0.38	0.39	0.38	0.36	0.37		
	P	scked Bulk Densit	y g)cm³	0.58	0.56	0.58	0.57	0.57	0.59		

	•	1	ABLE 5b					
			psule Deta					
5	Test	Run Numl 40	0er 41	42	43	44	45	5
	Moisture Content % w/w							
•	Powder when in the capsule	12.1	11.9	12.2	12.2	13.3	13.2	10
10	Capsule shell	13.9	14.2	13.3	13.5	13.1	13.0	10
	Total mg/capsule	11.8	11.9	11.9	11.6	11.6	11.5	
15	Emptying Test % w/w (See Example Ab)							15
	Mean	95.4	96.4	97.1	97.2	97.4	96.2	
20	Range	87.3-99.1	92.6-99.3	93.1-100	95.5-98.9	92.7-100	94.3-98.2	20
	Dispersion mg/capsule (See Example Ac)	5.32	4.03	4.74	4.97	4.28	3.12	
25	EXAMPLE 3 Pressure nozzle The trial was carried out using a spi This experiment was used to demo	ray drier hav	ing a main o	:hamber an	d a single c	yclone. providing	small	25
30	particles and establishing the order or mass mean diameter of less than 10 r of 6% w/v of aqueous sodium cromof of 120°C was used. The resulting pow- bulk density similar to that of microni	f magnitude nicrons. An glycate, an a der had part sed powder	of pressure stomiser pro ir inlet temp licles of size , but with a t	required to essure of 2. erature of 2 11 microns apped bulk) produce pi 1×10 ⁶ Kgm :30°C and ar : mass mear	rticles with -2, a feed co n air outlet t n diameter v	oncentration emperature with a particle	30
35	powder. The powder was satisfactory The appearance of the powder und with negligible fractured particles.	y in the capsi ler the light r	nicroscope	g test. was of unif	orm sphere:	s or collaps	ed spheres	35
40	EXAMPLE A The drug is dispensed from a gelatine capsule 6.4 mm in diameter and having two holes 0.8mm in diameter in a shoulder thereof mounted in a device (commercially available under the Registered Trade 10 Mark 'Spinhaler') according to British Patent No. 1,122,284 having a drawn wire shaft 2.03mm diameter 12,03mm diameter 13mm long and having an internal diameter of 2.08mm at its inner 13mm long and having an internal diameter of 2.08mm at its inner 15mm diameter of 15mm diameter of 2.08mm at its inner 15mm diameter 15mm d							40
45		illeria set oc		`				4!
50	(a) Dispersion test The filled capsules are mounted in dimensions set out immediately about two holes of 0.8mm diameter in a she delivered by the insufflator is determined to the described in British Patent Specification.	ve) of British oulder of the nined using a vion No. 1 08	n Patent Spe I capsule. Th I modified v 1.881. The n	cification N ne dispersion ersion of the nodification	on of the me e multistage as incorpora	dicament in e liquid imp ited in the p	the cloud singer present design	50
56	are the addition of an extra impinger mid-way along its length. The extra British Patent Specification No. 1,08	merit stage, a Implingemen 1,881 and co	and of a glas It stage was Insists essen In an effective	added prio stially of a je e cut-off of	r to the thre it of internal approximat	e stages de I diameter 2 ely 12 micro	scribed in 2.5cm and a ons at an air	5
	flow rate of 60 litres per minute. The jet of the extra stage. The insuffictor through at 60 litres per minute for 30 results are averaged. The weight of the analysis are averaged at the peper positioner.	glass tube, i is inserted in seconds. Ai the medicant disfler the fir	nto the upper least five conent collecte hal stage is dependent	nat diamete or, horizonti apsules are id on each s letermined appropriate	al end of the treated in the spectropho method).	glass tube nis manner impinger, o tometrical	and air drawn and the in the glass y after solution	64
	The particles disperse satisfactoril least 2.timg and most preferably at is stages and filter paper of the multi-s	ly if an averr east 6.0mg o	totel for a the particle	each capsu	IO OT ST ID SE	0.5 mg, pre sination of t	eferably at he last two	

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(b) Emptying test

The filled capsules are mounted in the capsule holder of the powder insufflator (having the specific dimensions set out above) of British Patent Specification No. 1,122,284 and pierced to produce two holes of 0.8mm diameter in a shoulder of the capsule. The insufflator is placed in a device adapted to suck air through 5 it for 2.5 seconds, the air flow rate at no time exceeding 60 litres per minute, and being held at 60 litres per minute for at least 2 seconds. The capsule mounted in the insufflator is subjected to 4 sucks as described and the weight of the material remaining in the capsule is determined. The above procedure is repeated 20 times

and the average of the results determined. The capsules empty satisfactorily if an average of at least 50%, preferably at least 75% and most preferably 10 at least 90% by weight of the material has emptied from each capsule.

(c) Dispersion

Single Stage Impingur

In a further refinement, the multistage liquid impinger of Example Aa) was simplified to give a single stage 15 liquid impinger, consisting of a single impingement assembly with a filter downstream. The impingement assembly consisted of a vertical jet of internal diameter 1.9cm and a collection plate of diameter 3.8cm. At the upper end, the jet was bent through an angle of 90° and the insufflator was attached to the distal end of this horizontal portion. The impingement characteristics of this single stage device were intended to be such that material reaching the filter of this device is similar in particle size to that reaching the final two stages 20 and filter of the multistage liquid impinger of Example As). The percentage of material reaching the filter of

the device is determined. In all samples of sodium cromoglycate prepared by the techniques exemplified above at least some of the particles were of toroidal (ring doughnut) shape.

25 CLAIMS

- 1. A finely divided inhalation drug comprising a therapeutically effective proportion of individual particles capable of penetrating deep into the lung, characterised in that a bulk of the particles which is both unagglomerated and unmixed with a coarse carrier, is sufficiently free flowing to be filled into capsules on 30 an automatic filling machine and to empty from an opened capsule in an inhalation device.
- 2. An inhalation drug in finely divided and unagglomerated form, wherein a substantial proportion of the individual drug particles have a spherical, collapsed spherical or ring doughnut shape.
- 3. A drug according to Claim 2 which contains sodium cromoglycate and wherein the particles are of ring doughnut shape.
- 4. A finely divided inhalation drug, wherein the permeametry: BET ratio, as hereinbefore defined, is in the range 0.5 to 1.0.
 - 5. A drug according to Claim 4, wherein the ratio is from 0.6 to 1.0.
 - A drug according to Claim 5, wherein the ratio is from 0.7 to 0.97.
- A drug according to any one of the preceding claims, wherein the particle density is from 1.3 to 1.7 g
- 40 cm³. 8. A drug according to Claim 7, wherein the particle density is from 1.3 to 1.6 g/cm³.
 - A drug according to any one of the preceding claims, having a loose bulk density of greater than 9. 0.3g/cm³.
 - 10. A drug according to Claim 9 having a loose bulk density of greater than 0.35g/cm³
- A drug according to Claim 10 having a loose bulk density of from 0.35 to 0.5g/cm³.
- 12. A drug according to any one of the preceding claims having a packed bulk density of from 0.4 to 0.75a/cm³.
- 13. A drug comprising sodium cromoglycate, wherein more than 90% of the drug particles are less than 60 microns in diameter and the drug has a loose bulk density of greater than 0.3g/cm³.
- 14. A drug comprising sodium cromoglycate, wherein more than 90% of the drug particles ae less than 60 microns in diameter and the drug has a packed bulk density of from 0.4 to 0.75g/cm³.
 - 15. A drug according to any one of the preceding claims, which is sodium cromoglycate and contains from 5 to 14% w/w of water.
 - 16. A drug according to Claim 15, which contains from 8 to 11% w/w water.
- 17. A drug according to any one of Claims 1 to 14, which is sodium cromoglycate and contains less than 55 1% w/w of water.
 - 18. A drug according to Claim 17, which contains less than 0.5% w/w of water.
 - 19. A drug according to any one of the preceding claims which comprises a mixture of sodium cromoglycate and a bronchodilator.
- 20. A drug according to any one of the preceding claims, wherein at least 50% of the drug particles are less than 60 microns in diameter.
 - 21. A drug according to Claim 20, whr _ in at least 50% of the drug particles are less than 40 microns in diameter.
 - 22. A drug according to Claim 21, wherein at least 50 % of the drug particles are less than 20 microns in

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diameter.

25. A drug according to any one of Claims 20 to 24, wherein more than 90% of the drug particles are of the diameter specified.

26. A drug according to any one of the preceding claims, wherein at least 50% of the particles are from 2 to 8 microns in diameter.

27. A drug according to any one of the preceding claims containing drug and water only. 28. A drug according to any one of Claims 1 to 26, wherein the individual particles contain both drug and 10 diluent.

29. A drug according to Claim 1 and substantially as hereinbefore described in any one of Examples 1 to 3.

30. A drug according to Claim 1 and substantially as shown in any one of Figures 1 to 10.

31. A capsule or cartridge which is filled to less than 80% by volume with a drug according to any one of 15 Claims 1 to 30.

32. A pharmaceutical formulation comprising a drug according to any one of Claims 1 to 30.

33. A process for the production of a finely divided drug according to any one of Claim 1, 2, 4, 13 or 14, which comprises atomising and drying a solution of the drug and collecting some or all of the particles which 20 are below 60 microns in diameter.

34. A process according to Claim 33, wherein the atomisation is effected by a two fluid nozzle atomiser or a syphon sprayer.

35. A process according to Claim 34, wherein the atomisation is effected by a two fluid pressure nozzle, a two fluid syphon nozzle or a two fluid sonic nozzle.

36. A process according to any one of Claims 33 to 35, wherein the atomisation and drying is carried out In a spray drying apparatus comprising an atomiser, a main chamber and at least one cyclone or bag filter.

37. A process according to any one of Claims 33 to 36, wherein the drug is sodium cromoglycate and the concentration of sodium cromoglycate in an aqueous solution to be dried is from 1 to 25% w/w.

38. A process according to Claim 37, wherein the concentration of sodium cromoglycate is from 5 to

30 20%. 39. A process according to Claim 38, wherein the concentration of sodium cromoglycate is from 10 to

15% w/v. 40. A process according to any one of Claims 23 to 39, wherein the air inlet temperature to the drying chamber is from 160° to 350°C, and the air outlet temperature is from 70° to 250°C.

41. A process according to Claim 33 and substantially as hereinbefore described in any one of Examples 35 1 to 3.

42. A drug produced by a process according to any one of Claims 33 to 41.

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